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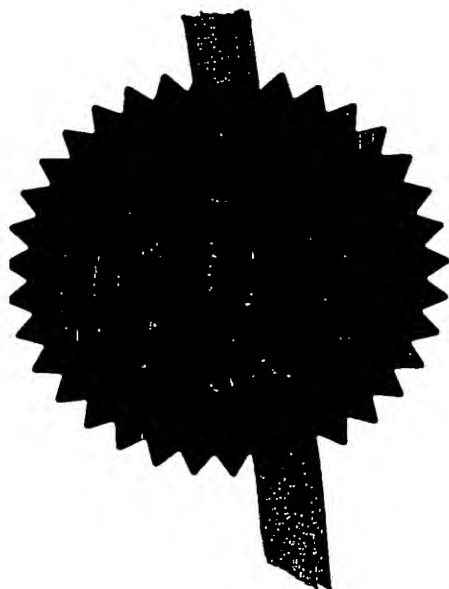
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P01/7700 0.00-0221942.6

2. Patent application number 20 SEP 2002

3. 0221942.6 and proprietor of the or of The University of Strathclyde  
each applicant (underline all surnames) ① McCance Building  
16 Richmond Street 79 84 9600 1  
Glasgow, G1 1XQ ①

Patents ADP number (if you know it) The University Court of the University of Glasgow  
Gilbert Scott Building  
If the applicant is a corporate body, give the University Avenue  
country/state of its incorporation ② Glasgow, G12 8QQ ② 773846003

4. Title of the invention Drug Delivery

5. Name of your agent (if you have one) Cruikshank & Fairweather  
"Address for service" in the United Kingdom 19 Royal Exchange Square  
to which all correspondence should be sent Glasgow  
(including the postcode) G1 3AE

Patents ADP number (if you know it) 547002

6. If you are declaring priority from one or more earlier patent applications, give the country and the date of filing of the or of each of these earlier applications and (if you know it) the or each application number	Country	Priority application number (if you know it)	Date of filing (day / month / year)
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7. If this application is divided or otherwise derived from an earlier UK application, give the number and the filing date of the earlier application	Number of earlier application	Date of filing (day / month / year)
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a) any applicant named in part 3 is not an inventor, or

b) there is an inventor who is not named as an applicant, or

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Description 24

Claim(s)

Abstract

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Statement of inventorship and right to grant of a patent (Patents Form 7/77)

Request for preliminary examination and search (Patents Form 9/77)

Request for substantive examination (Patents Form 10/77)

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Signature

Date

Cruikshank &amp; Fairweather 20 September 2002

12. Name and daytime telephone number of person to contact in the United Kingdom

Dr Paul Chapman 0141 221 5767

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DRUG DELIVERYField of Invention

5        This invention relates to the delivery of drugs. In particular, this invention relates to the oral delivery of poorly soluble drugs using novel amphiphilic polymers with both solubilising and absorption enhancing properties.

10

Background of Invention

      The oral delivery of poorly soluble drugs is usually accomplished with oil based formulations such as microemulsions (Dunn, C.J., Wagstaff, A.J., Perry, C.M., Plosker, G.L., Goa, K.L., 2001, Cyclosporin - An Updated Review of the Pharmacokinetic Properties, Clinical Efficacy and Tolerability of a Microemulsion-Based Formulation Neoral R(1) in Organ Transplantation, Drugs 61: 1257 - 2016; and Porter, C.J.H., Charman, W.N., 2001, In vitro Assessment of Oral Lipid Based Formulations, Advanced Drug Delivery Reviews 50: S127-S147) or low molecular weight surface active agents (BalandraudPieri, N., Queneau P.E., Caroli Bosc, F.X., BertaultPeres, P., Montet, A.M., Durand, A., Montet, J.C. 1997, Effects of Tauroursodeoxycholate Solutions on Cyclosporin and Bioavailability in Rats, Drug Metabolism and Disposition 25: 912-916; Guo, J.X., Ping, Q.N., Chen, Y. 2001, Pharmacokinetic Behaviour of Cyclosporin A in Rabbits by

Oral Administration of Lecithin Vesicle and Sandimmun  
Neoral, International Journal of Pharmaceutics 216: 17-  
21). Poorly soluble drugs are those drugs that are  
identified in the British Pharmacopoeia as "practically  
5 insoluble" (Medicines Commission, British Pharmacopoeia,  
The Stationary Office, London, 1998). Such drugs have an  
aqueous solubility of less than 0.1mg per millilitre of  
solvent (such as water) at a temperature of about 15°C -  
20°C.

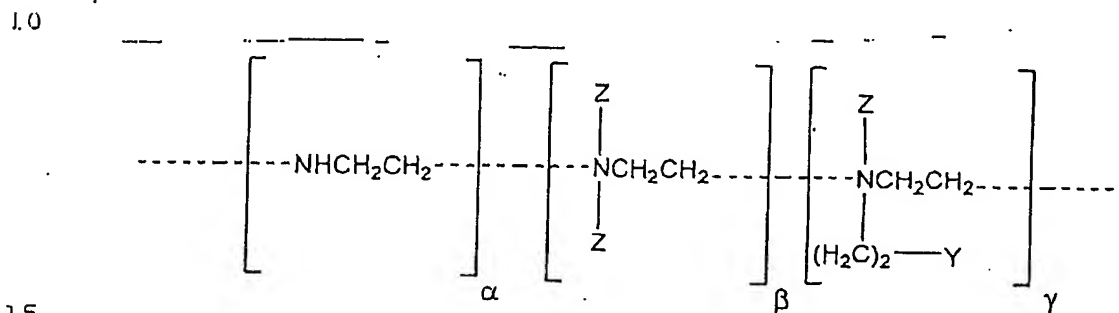
10 Previous attempts to promote oral absorption of  
poorly soluble drugs such as cyclosporin, have involved  
the use of oil and/or surfactant (Dunn, C.J., Wagstaff,  
A.J., Perry, C.M., Plosker, G.L., Goa, K.L., 2001,  
Cyclosporin - An Updated Review of the Pharmacokinetic  
15 Properties, Clinical Efficacy and Tolerability of a  
Microemulsion-Based Formulation Neoral R(1) in Organ  
Transplantation, Drugs 61: 957 - 2016; and Porter,  
C.J.H., Charman, S.A., Williams, R.D., Bakalova, M.B.,  
Charman, W.N., 1996, Evaluation of Emulsifiable Glasses  
20 for the Oral Administration of the Cyclosporin in Beagle  
Dogs, International Journal of Pharmaceutics 141: 227-  
237), bile salt (BaladraudPieri, N., Queneau, P.E.,  
CaroliBosc F.X., BertaultPeres, P., Montet, A.M., Durand,  
A., Montet, J.C., 1997, Effects of Tauroursodeoxycholate  
25 Solutions on Cyclosporin and Bioavailability in Rats, Drug  
Metabolism and Disposition 25:912-916), phospholipid  
based systems (Guo, J.X., Ping, Q.N., Chen, Y., 2001,  
Pharmacokinetic Behaviour of Cyclosporin A In Rabbits by  
Oral Administration of Lecithin Vesicle and Sandimmun

- Neoral, International Journal of Pharmaceutics 21: 17 - 21; and Leigh, M., Hoogevest, P.V., Tiemmessem, H., 2001 Optimising the Oral Bioavailability of the Poorly Water Soluble Drug Cyclosporin A Using Membrane Lipid Technology, Drug Delivery and Sciences 1: 73-77) or cyclodextrins (Miyake, K., Arima, H., Irie, T., Hirayama, F., Uekama, K., 1999, Enhanced Absorption of Cyclosporin A by Complexation with Dimethyl-Beta-Cyclodextrin in Bile duct-Cannulated and Non-Cannulated Rats, Biological and Pharmaceutical Bulletin 22: 66-72). Although a nanocapsule formed during in-situ polymerisation has also been proposed for cyclosporin delivery, this technique has difficulties in delivering the drug (Bonduelle, S., Carrier, M., Pimienta, C., Benoit, J.P., Lenaerts, B., 1996, Tissue Concentration of Nanoencapsulated Radiolabelled Cyclosporin Following Peroral Delivery in Mice or Ophthalmic Application in Rabbits, European Journal of Pharmaceutics and Biopharmaceutics, 42: 31 - 319).
- 20 Cyclosporin is a lipophilic immunosuppressant used to treat transplant and autoimmune disease patients. Cyclosporin is poorly soluble in a variety of solvents and is currently administered as a micro-emulsion formulation.
- 25 It is an object of embodiments of the present invention to obviate or mitigate at least one or more of the aforementioned problems.

It is a further object of embodiments of the present invention to improve delivery of poorly soluble drugs to a recipient.

## 5 Summary of the Invention

According to a first aspect of the present invention there is provided a polyethylenimine polymer according to the following formula:



wherein  $\alpha$  is between 0 to 90%;

$\beta$  is between 0 to 100%;

20  $\gamma$  is between 0 to 50%;

wherein  $\alpha + \beta + \gamma = 100\%$ ; and

the Z groups are hydrophobic and are independently hydrogen or any linear or branched, substituted or unsubstituted, or cyclo form of any hydrophobic  
25 substituent; and

Y may represent a hydrophilic substituent.

It should be understood that the monomer units identified with  $\alpha$ ,  $\beta$  and  $\gamma$  may form any arrangement in the

polyethylenimine polymer. The arrangement of the  $\alpha$ ,  $\beta$  and  $\gamma$  units may therefore be random or in a block copolymer form such as  $\alpha\beta\gamma\alpha\beta\gamma$  etc. This is identified above by the dashed line between the different monomer  
 5 units.

The polyethylenimine polymer may be linear or branched.

The ratios for  $\alpha$ ,  $\beta$ ,  $\gamma$  are numerical ratios.

Typically, the Z groups may independently be  
 10 selected from any of the following hydrophobic substituents: an alkyl, an alkenyl, and alkynyl, an aryl, an acyl, a hydroxy alkyl, a hydroxy acyl, polyethylene glycol or any sugar.

The Z groups may independently be any linear or  
 15 branched, substituted or unsubstituted, or cyclo form of the following alkyl, alkenyl, alkynyl, aryl, acyl, hydroxy alkyl, hydroxy acyl, polyethylene glycol or any sugar groups:  $C_1 - C_{10}$ ;  $C_1 - C_{12}$ ;  $C_1 - C_6$  or  $C_1$ .

The Z groups may be  $C_1 - C_6$  linear alkyl groups.

20 Y may represent any of the following:  $-NH_2$ ;  $-NHA$ ;  $N'R_1R_2R_3$ ; and  $-N'R_1R_2A$ .

$R_1$ ,  $R_2$ , or  $R_3$  may be selected from any of the following substituents: an alkyl, an alkenyl, an alkynyl, an aryl, an acyl, a hydroxy alkyl, a hydroxy acyl,  
 25 polyethylene glycol or any sugar.

$R_1$ ,  $R_2$  and  $R_3$  may independently be any linear or branched, substituted or unsubstituted, or cyclo form of the following alkyl, alkenyl, alkynyl, aryl, acyl,

hydroxy alkyl, hydroxy acyl, polyethylene glycol or any sugar groups:  $C_1 - C_{11}$ ;  $C_1 - C_{12}$ ;  $C_1 - C_6$  or  $C_1$ .

Typically,  $R_1$ ,  $R_2$  and  $R_3$  are  $C_1 - C_6$  linear alkyl groups.

5 All of  $R_1$ ,  $R_2$  and  $R_3$  may be  $CH_3$ .

Conveniently there may be between 1 and a maximum of 3  $R$  substituents on any single nitrogen. This allows for primary, secondary and tertiary amines.

The groups  $A$  may be selected from any of the  
10 following linear or branched, substituted or unsubstituted, or cyclo groups:  $C_1 - C_{10}$ ;  $C_3 - C_{24}$ ; or  $C_{12} - C_{16}$ .

Typically, the groups  $A$  may be a linear  $C_{12} - C_{16}$  alkyl group.

15 In particular,  $A$  may be  $CH_3(CH_2)_{15}$ .

The ratio of quaternary ammonium nitrogens to nitrogens of amino groups may be selected from any of the following: 0.01% - 100%; 10% - 90%; 30% - 70%; 40% - 60%; 50% - 90% or 60% - 80%. The preferred range is 40%  
20 - 90%. A high proportion of quaternary ammonium groups promotes solubilisation of both the polyethylenimine polymer and a hydrophobic drug.

The parent polyethylenimine compound used to make the polyethylenimine polymer may have an average  
25 molecular weight of about 2 - 50kD, or more particularly, of about 10 - 25 kD.

The polyethylene polymer may have an average molecular weight of about 10 - 25 kD.

The polyethylenimine polymer may produce hydrophobic domains. Hydrophobic domains are areas of the molecule's self-assembly where hydrophobic compounds or compounds which are poorly soluble in water are able to reside and thus become solubilised with an aqueous disperse phase. The level of hydrophobic modification may be from 0.01 - 50%, 0.1 - 20% or 1 - 10% of amino groups. The preferred level of hydrophobic modification is 1 - 10% of amino groups.

10 All possible monomeric subunits in accordance with the structure as defined in formula I are shown in Figure 1:

wherein m is between 0 - 90 %;

n is between 0 - 100 %;

15 p is between 0 - 50 %;

q is between 0 - 50 %;

u is between 0 - 50 %;

v is between 0 - 50 %;

w is between 0 - 20 %;

20 x is between 0 - 20 %;

y is between 0 - 20 %; and

z is between 0 - 20 %;

wherein,  $m + n + p + q + u + v + w + x + y + z = 100\%$ ; and

25 A, R<sub>1</sub>, R<sub>2</sub>, R<sub>3</sub> and Z are as defined above.

It should be appreciated that the monomer units m, n, p, q, u, v, w, x, y and z may be arranged in any order.

The ratios for m, n, p, q, u, v, w, x, y and z are numerical ratios.

Typically, if  $m = 0\%$  then n is not equal to  $0\%$ .

Typically, if  $n = 0\%$  then m is not equal to  $0\%$ .

5 Typically, if  $p = 0\%$  then  $q + u + v + w + x + y + z$  does not equal  $0\%$ .

Typically, if  $q = 0\%$  then  $p + u + v + w + x + y + z$  does not equal  $0\%$ .

Typically, if  $u = 0\%$  then  $p + q + v + w + x + y + z$  10 does not equal  $0\%$ .

Typically, if  $v = 0\%$  then  $p + q + u + w + x + y + z$  does not equal  $0\%$ .

Typically, if  $w = 0\%$  then  $x + y + z + n$  does not equal  $0\%$ .

15 Typically, if  $x = 0\%$  then  $w + y + z + n$  does not equal  $0\%$ .

Typically, if  $y = 0\%$  then  $w + x + z + n$  does not equal  $0\%$ .

Typically, if  $z = 0\%$  then  $w + x + y + n$  does not 20 equal zero.

Conveniently,  $m + n$  lies between 50 to 100%.

Conveniently,  $p + q + u + v$  lies between 20 to 50%.

Conveniently,  $w + x + y + z$  lies between 0.01 to 10%.

25 It is possible that polyethylenimine may be linear ( $n=100$ ) or branched as shown in Figure 1. If  $n = 0\%$ , however, then m must be equal to a value greater than  $0\%$  as this allows for the branched material with no backbone quaternisation on erstwhile secondary amines.

It is possible that p, q, u, v, w, x, y or z may be equal to 0%. However, the sum total of p, q, u, v, w, x, y and z may be equal to a value greater than 0%, as this allows for the branched compound to be included.

5 Alternatively, w, x, y or z may be equal to 0%. However, the sum total of w, x, y or z may not be equal to 0%. This allows for a hydrophobically substituted branched compound.

Typically,  $m + n = 60\%$ ,  $w + x + y + z = 6\%$ , and  $p +$   
10  $q + u + v = 34\%$ . Using these ranges defines the quaternary ammonium cetyl polyethylenimine found in the Example Section of the present application.

According to a second aspect of the present invention there is provided a method of forming a  
15 polyethylenimine polymer according to the first aspect by reacting a polyethylenimine compound formed from the polymerisation of ethylenimine with a first organo halide to form an organo side chain on the polyethylenimine compound, and then a second organo halide to react with  
20 an amino group on the polyethyleneimine compound.

The ethylenimine used may be branched or linear.

Branched polyethylenimine may be prepared by the acid catalysed polymerisation of, for example, aziridine (ethylenimine) (Dick, C.R., Ham, G.E., J. Macromol. Sci. 25 1970, A4, 1301-1314; von Harpe, A., Petersen, H., Li, Y., Kissel, T., J. Control. Rel., 2000, 69, 309-332). Linear polymers may be prepared by controlling the conditions of ethylene polymerisation (Zhuk, D.S., Gembitsky, P.A., Alexandrovich, A.I., US Patent No. 4,032,480).

The first organo halide may be any linear or branched, substituted or unsubstituted, or cyclo form of any alkyl, alkenyl, alkynyl, aryl or acyl halide or any hydrophilic halide. The halide may be any of fluoride, chloride, bromide or iodide.

The organo group of the first organo halide may be selected from any of the following linear or branched, substituted or unsubstituted, or cyclo groups:  $C_1 - C_{30}$ ;  $C_6 - C_{24}$ ; or  $C_{12} - C_{18}$ .

Typically, the first organo halide is a linear  $C_{12} - C_{18}$  alkyl halide.

In particular, the first organo halide may be cetyl bromide (e.g.  $CH_3(CH_2)_{14}Br$ ).

The second organo halide may be any alkyl, alkenyl, alkynyl, aryl or acyl halide or any hydrophilic halide. The halide may be any of fluoride, chloride, bromide or iodide.

The organo group of the second organo halide may be selected from any of the following linear or branched, substituted or unsubstituted, or cyclo groups:  $C_1 - C_{30}$ ;  $C_6 - C_{24}$ ; or  $C_{12} - C_{18}$ .

Typically, the second organo halide is a linear  $C_1 - C_6$  alkyl halide. In particular, the second organo halide may be methyl iodide.

The polyethylenimine compound and first organo halide may be mixed in an organic solvent such as tetrahydrofuran, which may then be refluxed. The refluxing may occur in an alcoholic solution of, for example, sodium hydroxide. Cetyl polyethylenimine may

then be isolated and may then be reacted with the second organo halide.

The second organo halide may be added in the presence of, for example, a metal hydroxide (e.g. sodium hydroxide), a metal halide (e.g. sodium iodide) and an alcohol (e.g. methanol).

The polyethylenimine polymer may then be obtained by washing, dialysis and using an ion exchange column.

Further quaternisation may be obtained by adding more of the second organo halide.

The formed polyethylenimine polymer may be that as represented in Figure 1.

It is also possible to prepare a substituted linear polyethylenimine with the end nitrogens protected, subsequently deprotect the terminal amines and then attach this substituted linear polyethylenimine to the branched molecule and follow the whole conjugation step with a quaternary ammonium step.

According to a third aspect of the present invention there is provided a composition comprising a polyethylenimine polymer according to the first aspect and a pharmaceutically acceptable carrier.

Pharmaceutically acceptable carriers are well known to those skilled in the art and include, but are not limited to, 0.1 M and preferably 0.05 M phosphate buffer or 0.9% w/v saline. Additionally, such pharmaceutically acceptable carriers may be aqueous or non-aqueous solutions, suspensions, and emulsions. Examples of non-aqueous solvents are propylene glycol, polyethylene

glycol, vegetable oils such as olive oil, and injectable organic esters such as ethyl oleate. Aqueous carriers include water, alcoholic/aqueous solutions, emulsions or suspensions, including saline and buffered media.

5 Parenteral vehicles include sodium chloride solution, Ringer's dextrose, dextrose and sodium chloride, lactated Ringer's or fixed oils. Preservatives and other additives may also be present, such as, for example, antimicrobials, antioxidants, chelating agents, inert

10 gases and the like.

Typically, the ratio of polyethylenimine polymer to pharmaceutically acceptable carrier ranges from any of the following: 0.0001 - 100 w.v., 0.005 - 50 w.v.; 0.001 - 30 w.v.; 0.001 - 10 w.v.; or 0.01 - 1 w.v.

15 According to a fourth aspect of the present invention there is provided a pharmaceutical composition comprising a polyethylenimine polymer according to the first aspect and a drug.

The drug may be poorly soluble in aqueous solvents

20 such as water. The drug may be administered to a patient as a solution or a particulate formulation.

The drug may be selected from any of the following: cyclosporin; steroids such as prednisolone, oestradiol, testosterone; drugs with multicyclic ring structures

25 which lack polar groups such as paclitaxel; and drugs such as etoposide.

Typically, the ratio of the polyethylenimine polymer to the drug may be selected from any of the following: 0.001 - 100%; 0.1 - 100%; 1 - 100%; 10 - 90%; 30 - 70%.

The pharmaceutical composition may also comprise a pharmaceutically acceptable carrier.

Typically, the ratio of polyethylenimine polymer to drug to pharmaceutically acceptable carrier may be in the range of 5 - 20mg : 0.5 - 5mg : 0.5 - 5mL or 5 - 20mg : 0.5 - 5mg : 0.5 - 5g. In particular, the ratio of polyethylenimine polymer to drug to pharmaceutically acceptable carrier may be about 10mg:2mg:1mL or about 10mg:2mg:2g:

10 The pharmaceutical composition may be in the form of any of the following: tablets, suppositories, liquid capsule powder form, or a form suitable for pulmonary delivery.

When tablets are used for oral administration, typically used carriers include sucrose, lactose, mannitol, maltitol, dextran, corn starch, typical lubricants such as magnesium stearate, preservatives such as paraben, sorbin, antioxidants such as ascorbic acid,  $\alpha$ -tocopherol, cysteine, disintegrators or binders. When administered orally as capsules, effective diluents include lactose and dry corn starch. A liquid for oral use includes syrup, suspension, solution and emulsion, which may contain a typical inert diluent used in this field, such as water. In addition, sweeteners or  
25 flavours may be contained.

Suppositories may be prepared by admixing the compounds of the present invention with a suitable non-irritative excipient such as those that are solid at normal temperature but become liquid at the temperature

in the intestine and melt in rectum to release the active ingredient, such as cocoa butter and polyethylene glycols.

The dose of the polymer can be determined on age, body weight, administration time, administration method, combination of drugs, the level of condition of which a patient is undergoing therapy, and other factors. While the daily does may vary depending on the conditions and body weight of patients, the species of active ingredient, and administration route, in the case of oral use, the daily does may be about 0.1 - 100 mg/person/day, preferably 0.5 - 30 mg/person/day.

According to a fifth aspect of the present invention there is provided a method of dissolving poorly soluble drugs suitable for oral delivery, using a preformed polymer.

By preformed polymer herein is meant a polymer which already exists and does not need to be formed during an in-situ polymerisation step.

The preformed polymer may be a polyethylenimine polymer according to the first aspect.

The poorly soluble drug may be selected from any of the following: cyclosporin; steroids such as prednisolone; oestradiol; testosterone; drugs with multicyclic ring structures which lack polar groups such as paclitaxel; drugs such as etoposide.

The fact that  $R_1$ ,  $R_2$ ,  $R_3$  and  $R_4$  may be long chain alkyl groups or other hydrophobic groups makes it possible for the polyethylene polymer according to the

first aspect to dissolve poorly soluble drugs in aqueous media.

The preformed polymer may also be used to dissolve polar (aqueous soluble) materials within hydrophobic media.

According to a sixth aspect of the present invention there is provided use of a preformed polymer according to the fifth aspect in dissolving poorly soluble drugs in the preparation of a composition.

10 The composition may be a pharmaceutical composition comprising a drug and/or a pharmaceutically acceptable carrier.

#### Brief Description of the Drawings

15 Embodiments of the present invention will now be described, by way of example only, with reference to the accompanying drawings in which:

Figure 1 is a representation of a polyethyleneimine polymer formed according to the present invention;  
20 and

Figure 2 is a Transmission Electron Microscopy (TEM) image of quaternary ammonium cetyl polyethyleneimine (QCPEI2) and cyclosporin nanoparticles.

25

### Examples

#### Example 1 - Synthesis of Quaternary Ammonium Cetyl Polyethylenimine (QCPEI)

Alkylation of polyethylenimine was carried out according to a previously reported method (Noding, G., Heitz, W., 1996. Amphiphilic Polyethylenimines Based on Long-Chain Alkyl Bromide Macromolecular Chemistry and Physics 199: 637 - 1644). Briefly, polyethylenimine ( $M_w = 25kD$ , 5g) was alkylated by refluxing with cetyl bromide (1.8g) and tetrahydrofuran (50ml) for 48 hours, followed by the addition of an alcoholic solution of sodium hydroxide (4.8g in 25ml methanol), and a further reflux period of 24 hours. Sodium bromide was removed by filtration and the product isolated by evaporation of the solvent, exhaustive dialysis and freeze-drying. 0.6g of cetyl polyethylenimine was then quaternised by reaction with methyl iodide (2.6ml) in the presence of sodium hydroxide (0.23g), sodium iodide (0.28g) and methanol (100ml) for 3 hours at 36°C. The product was isolated by precipitation in ether (400ml), washing with ethanol, exhaustive dialysis of an ethanolic solution and elution through an ion exchange column to isolate the hydrochloride salt.

A yellow cotton wool like solid which is the quaternary ammonium cetyl polyethyleneimine (QCPEI1) was obtained on freeze drying.

A further quaternisation of quaternary ammonium cetyl polyethyleneimine (QCPEI1) produced a doubly

quaternerised compound, i.e. di-quaternary ammonium cetyl polyethylenimine (QCPEI2).

## Characterisation of Quaternary Ammonium Cetyl

### 5 Polyethylenimine

<sup>1</sup>H NMR and <sup>1</sup>H correlation spectroscopy as well as <sup>13</sup>C NMR experiments (Bruker, AMX 400 MHz spectrometer, Bruker Instruments UK) were carried out on the quaternary cetyl polyethylenimine in deuterated methanol. Elemental  
10 analysis was carried out on the products using a Perkin Elmer 2400 analyser.

### Polymer Aggregation

The aggregation of an aqueous solution of the  
15 polymers was studied using a pyrene probe for hydrophobic domains (see Kalyanasundaram, K., Thomas, J.K., 1977, Environmental Effects on the Vibronic Band Intensities in Pyrene Monomer Fluorescence and the Application to Studies of Micellar Systems, Journal of the American  
20 Chemical Society 99: 2035 - 2044). Fluorescence scans (excitation = 340nm) were performed on various concentrations of the polymer dissolved in an aqueous pyrene solution (2µM). The ratio of the intensity of the third and first peaks ( $I_3/I_1$ ) was used to assess the  
25 hydrophobicity of the pyrene environment which is an indirect probe for polymer association.

Polymer aggregation was also assessed by recording the hypsochromic shift in the UV absorption spectrum of

methyl orange (Lieske, A., Jaeger, W., 1999, Block Copolymers Containing Polysoap Blocks, Tenside Surfactants Detergents 36: 155 - 161) in 25 $\mu$ M in 0.02M borate buffer when encapsulated within a hydrophobic environment. UV absorption scans (300 - 600nm) were performed on various concentrations of the polymer dissolved in the methyl orange-borate solution and the wavelength of maximum absorbance noted.

TABLE 1: Quaternary ammonium cetyl polyethyleneimine (QCPEI1) aggregation in aqueous solution as measured by the increase in ( $I_3/I_1$ ) ratio in the pyrene fluorescence and by the hypsochromic shift in the methyl orange spectra

QCPEI1 I <sub>3</sub> /I <sub>1</sub> ratio (QCPEI1 concentration in mg mL <sup>-1</sup> )	QCPEI1 Methyl Orange wavelength of maximum absorbance (QCPEI1 concentration in mg mL <sup>-1</sup> )	QCPEI2 I <sub>3</sub> /I <sub>1</sub> ratio (QCPEI2 concentration in mg mL <sup>-1</sup> )	QCPEI2 Methyl Orange wavelength of maximum absorbance (QCPEI2 concentration in mg mL <sup>-1</sup> )
0.64 (0)	465 (0)	0.61 (0)	465 (0)
0.88 (0.27)	456 (0.50)	0.823 (0.21)	456 (0.55)
0.89 (1.72)	452 (1.52)	0.862 (1.621)	450 (1.63)
0.92 (3.72)	452 (3.73)	0.871 (3.24)	456 (3.70)
0.98 (7.04)	454 (7.80)	0.853 (4.37)	455 (7.85)
		0.926 (6.49)	456 (14.25)

The synthesis of the cetyl polyethylenimine was confirmed by a proton NMR and assignments were made as follows:

$\delta = 0.87 = \text{CH}_3$  (cetyl),  $\delta 1.25 = \text{CH}_2$  (cetyl),  $\delta 1.45 = \text{CH}_2 - \text{N}$  (cetyl),  $\delta 2.7 - 2.8 = \text{CH}_2 - \text{N}$  (cetyl and

polyethylenimine). Quaternisation of cetyl polyethylenimine to produce quaternary ammonium cetyl polyethylenimine was confirmed by  $^{13}\text{C}$  NMR  $\delta 14.6 = \text{CH}_3(\text{cetyl})$ ,  $\delta 23.9 = \text{CH}_2(\text{cetyl})$ ,  $\delta 52.5$  and  $54.8 = \text{CH}_2(\text{CH}_2\text{N}^+)$ ,  $\delta 59.8$  and  $63.5 = \text{CH}_2\text{N}$  and  $\text{CH}_2\text{N}^+(\text{polyethylenimine})$  and  $^1\text{H}$  NMR  $\delta 0.90 = \text{CH}_3(\text{cetyl})$ ,  $\delta 1.3 = \text{CH}_2(\text{cetyl})$ ,  $\delta 1.47 = \text{CH}_2(\text{cetyl})$ ,  $\delta 1.85 = \text{CH}_2 - \text{N}(\text{cetyl})$ ,  $\delta 2.5 - 4.7 = \text{CH}_2\text{N}$ ,  $\text{CH}_2\text{N}^+$  and  $\text{CH}_2\text{N}^+$ .

The yields of cetyl polyethylenimine, quaternary polyethylenimine (QCPEI1) and di-quaternary cetyl polyethylenimine (QCPEI1) were 67%, 85% and 46%, respectively.

The degree of cetylation was found to be 5.2% of all amine groups using elemental analysis data. The degree of conversion of amines to quaternary ammonium moieties was approximately 64% for quaternary cetyl polyethylenimine and 81% for di-quaternary cetyl polyethylenimine.

Both quaternary ammonium polymers aggregate to produce hydrophobic domains in aqueous solution (See Table 1). This is shown by the increase in the I3/I1 values and also by the shift to a lower wavelength of the methyl orange peak. These hydrophobic domains serve to solubilise poorly aqueous soluble (hydrophobic) drugs such as cyclosporin; in the case of the less quaternised variant - QCPEI1 which forms a clear micellar liquid with cyclosporin, when freshly prepared (Table 1), effectively encapsulating cyclosporin within the hydrophobic domains.

Example 2 - Preparation of Quaternary Cetyl  
Polyethylenimine - Cyclosporin Formulations

Quaternary cetyl polyethylenimine polymers were  
5 dissolved by probe sonication on ice (Soniprep  
Instruments, UK) followed by the addition of cyclosporin,  
which was incorporated into the polymer solution by probe  
sonication. Formulations were stored for up to 13 days  
and observed for particle formation. Particulate  
10 formations were sized by photon correlation spectroscopy,  
imaged by both transmission electron microscopy (TEM)  
with negative staining (see Wang, W., Tetley, L.,  
Uchegbu, I.F., 2001. The Level of Hydrophobic  
Substitution and the Molecular Weight of Amphiphilic  
15 Poly-L-Lysine-based Polymers Strongly Affects Their  
Assembly into Polymeric Bilayer Vesicles, Journal of  
Colloid and Interface Science 237: 200-207) and freeze  
fracture electron microscopy (see Uchegbu, I.F.,  
Schatzlein, A.G., Tetley, L., Gray, A.I., Sludden, J.,  
20 Siddique, S., McSha, E., 1998, Polymeric Chitosan - Based  
Vesicles for Drug Delivery, Journal of Pharmacy and  
Pharmacology 50: 453-458). Clear micellar formulations  
were filtered with a 0.45µm filter and the filtered  
formulations assayed by HPLC using a reverse phase Waters  
25 Spherisorb ODS column (25cm x 4.6mm), eluted with a  
water, acetonitrile tert-butyl methyl ether,  
orthophosphoric acid (350:600:50:1). Detection was by  
UV (λ=210nm).

Table 2: QCPEI-cyclosporin formulations

Formulation	Initial Appearance	Initial Mean Particle Size (nm)	Recovery of cyclosporin from micellar solutions (a)		Mean Particle Size (nm)	
			Freshly prepared (mean $\pm$ s.d.)	After storage (2-8°C) for 90 days (mean $\pm$ s.d.)	Storage (2-8°C) for 4 days followed by exposure to room temperature for 15 min	Storage (2-8°C) for 3 days followed by exposure to 37°C for 15 min
QCPEI1	Clear liquid	-	78.7 $\pm$ 3.14 (n=3)	83.3 $\pm$ 6.60 (n=4)	552 (n=3)	608 (n=6)
QCPEI2	Colloidal	310 (n=4)	-	-	377 (n=1)	512 (n=3)

(a) Initial Concentration = 2mg mL<sup>-1</sup>

n Denotes number of formulations assayed.

(In Table 2 the blank boxes (represented with a "-") represent particulate formulations, which cannot be assayed in the same way as micellar formulations).

As shown in Table 1 both quaternary ammonium polymers (i.e. QCPEI1 and QCPEI2) aggregate to produce hydrophobic domains in aqueous solutions. These hydrophobic domains serve to solubilise cyclosporin. In the case of the less quaternised variant - QCPEI1 forms a clear micellar liquid with cyclosporin, when freshly prepared, effectively encapsulating cyclosporin within hydrophobic domains. However, as shown in Table 2, the polymer exhibits a lower critical solution temperature and becomes less hydrated with increase in temperature resulting in aggregation of the polymeric micelles to form nanoparticles. Furthermore, Table 2 shows storage of QCPEI1 at refrigeration temperature preserved the micellar formulation. The micellar formulation is preserved as analysis of the optically clear samples after storage for 90 days shows that there is no precipitation of cyclosporin.

In contrast to QCPEI1, the doubly quaternarised compound QCPEI2, which is less water soluble than QCPEI1 initially formed stable nanoparticles with cyclosporin. Figure 2 shows that the double quaternarised compound (QCPEI2) does not form micelles with cyclosporin. The size bar shows that the aggregates formed are too large to be micelles although the image could show an aggregate of lots of micelles. These will still be technically nanoparticles as the formulation is not optically clear.

Although the polymer forms micelles within which cyclosporin is solubilised, the polymer exhibits a lower critical solution temperature and becomes less hydrated with increase in temperature resulting in aggregation of the polymeric micelles to form nanoparticles after exposure to elevated temperatures (i.e. removal from the fridge, Table 2). However, storage of QCPEI1 at refrigeration temperature preserved the micellar formulation (Table 2) and there was no conversion of the micelles into nanoparticles. In contrast to QCPEI1, the doubly quaternised compound QCPEI2, which is less water soluble than QCPEI1, initially formed stable nanoparticles with cyclosporin (Figure 2, Table 2) and does not form the micelles with cyclosporin.

### Example 3 - Oral Administration of Quaternary Cetyl Polyethylenimine-Cyclosporin Formulations

Groups of male Wistar rats (n=4 i.e. the group size, weight = 200 - 220g) were fasted for 12 hours before

dosing and subsequently dosed intragastrically (10mg kg<sup>-1</sup>) with an optically clear quaternary cetyl polyethylenimine (QCPEI1) - cyclosporin formulation (10:2); a particulate quaternary cetyl polyethylenimine (QCPEI2) - Cyclosporin (10:2) formulation; Neoral (Registered Trademark) or water. Neoral is a microemulsion formulation of cyclosporin manufactured and marketed by Novartis.

Blood was taken from the tail vein of these anaesthetised rats at 1 hour, 4 hours and 24 hours after dosing. Plasma was separated by centrifugation at 1000g and stored at -20°C until analysis could be performed on the samples. Cyclosporin was measured in the plasma samples using a monoclonal antibody radioimmunoassay kit (Cyclo-Trac SP-Whole Body Radioimmunoassay Kit) supplied by Diasorin, UK.

Table 3: Blood Levels Following Oral Cyclosporin Dosing

Time	Formulations		
	ngL <sup>-1</sup> of cyclosporin in blood		
	Neoral ®	QCPEI1	QCPEI2
1h	1525±267*	583±284	748±482
4h	1321±163	1179±360	1387±539
24h	346±37	315±95	295±45

\* = statistically significant difference between groups at the same time point (p<0.05)

The oral QCPEI1 formulations were well tolerated in rats with no gross adverse events recorded. Plasma levels

at the 4 hour time point from the oil free QCPEI formulations were indistinguishable from peak levels obtained using Neoral (Registered Trademark), although Neoral (Registered Trademark) was absorbed faster than the QCPEI formulations shown in Table 3. The amphiphilic polyethyleneimine polymer therefore promotes the absorption of a poorly soluble drug such as cyclosporin.

Within the 37°C environment of the gut lumen it is assumed, although not wishing to be bound by theory, that the narrow particle formulation prevails for both polymers and that these nanoparticles experience the gradual loss of cationic micellar aggregates still encapsulating their hydrophobic payload. As cationic polymers are known to facilitate transport across epithelial membranes and across cell membranes, these micellar aggregates may also facilitate the intestinal absorption of cyclosporin. The disassociation of the nanoparticle into single micellar aggregates results in the delayed absorption when compared to the oil containing formulation.



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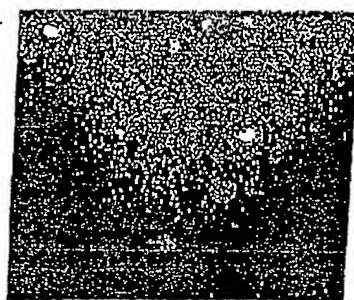


Figure 2: TEM of QCPEI2, cyclosporine (10: 2) nanoparticles, bar = 200nm

PCT Application

**GB0304036**



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